

Regularized D-bar method for electrical impedance tomography

$$\frac{\partial}{\partial \bar{k}} \mu_R(x, k) = \frac{t_R^{\text{exp}}(k)}{4\pi \bar{k}} e^{-i(kx + \bar{k}\bar{x})} \overline{\mu_R(x, k)}$$

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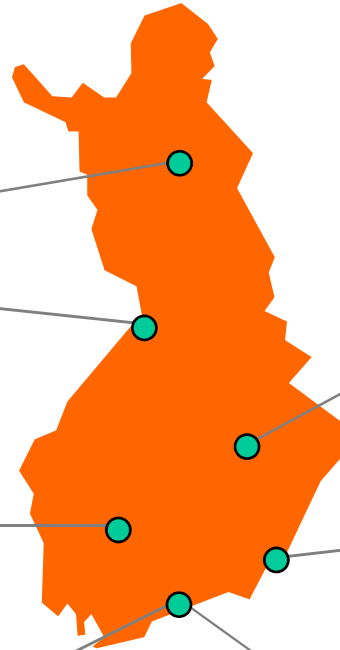
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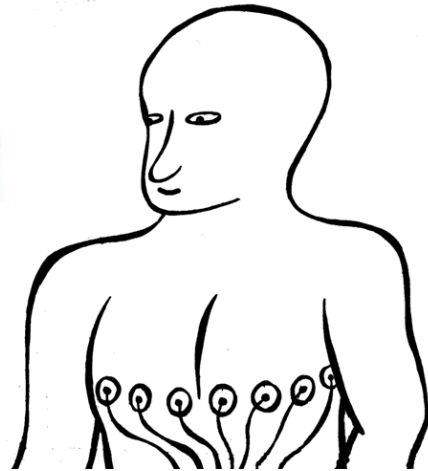
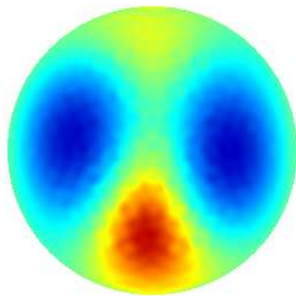
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1. Electrical impedance tomography

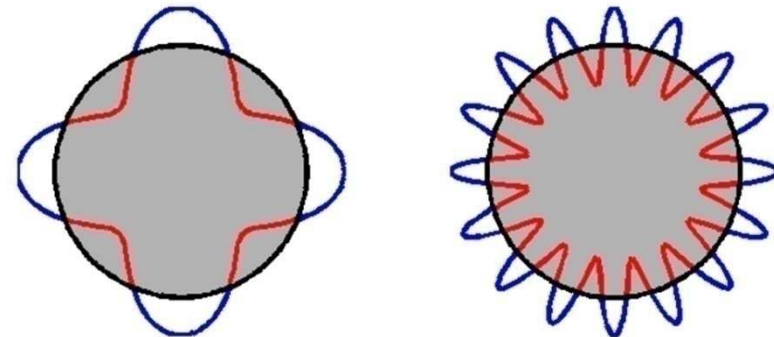
$$\frac{\partial}{\partial \bar{k}} \mu(x, k) = \frac{t(k)}{4\pi \bar{k}} e^{-i(kx + \bar{k}\bar{x})} \overline{\mu(x, k)}.$$

2. Theory of the D-bar method

3. Regularization results

$$\sup_{\Lambda_\gamma^\varepsilon} \left\{ \|\Gamma_{\alpha(\varepsilon)} \Lambda_\gamma^\varepsilon - \gamma\|_{L^\infty(\Omega)} : \|\Lambda_\gamma^\varepsilon - \Lambda_\gamma\|_Y \leq \varepsilon \right\}$$

4. Practical computation

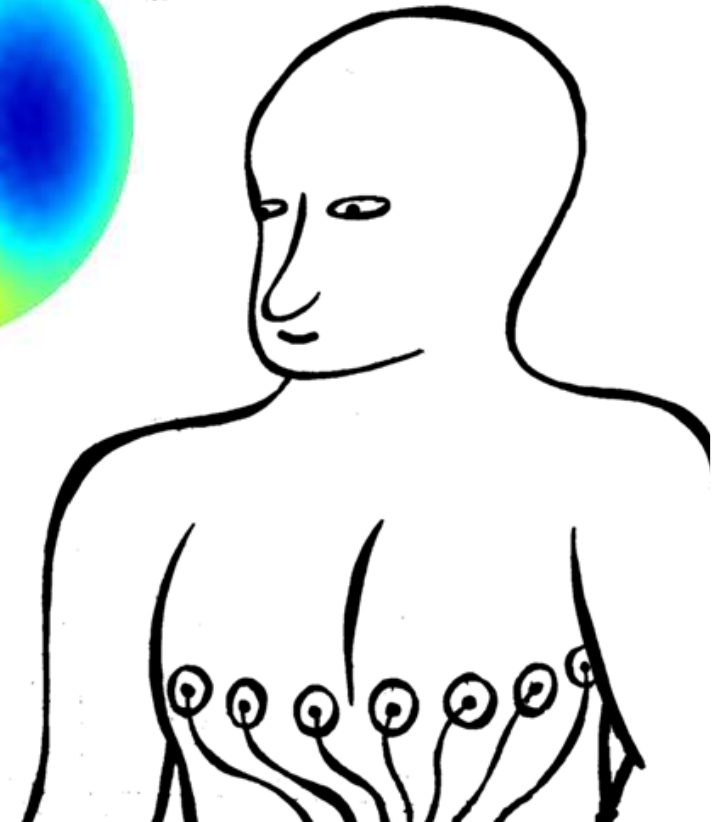
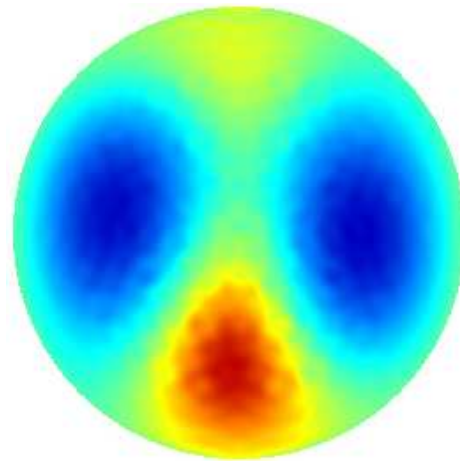


Electrical impedance tomography (EIT) is an emerging medical imaging method

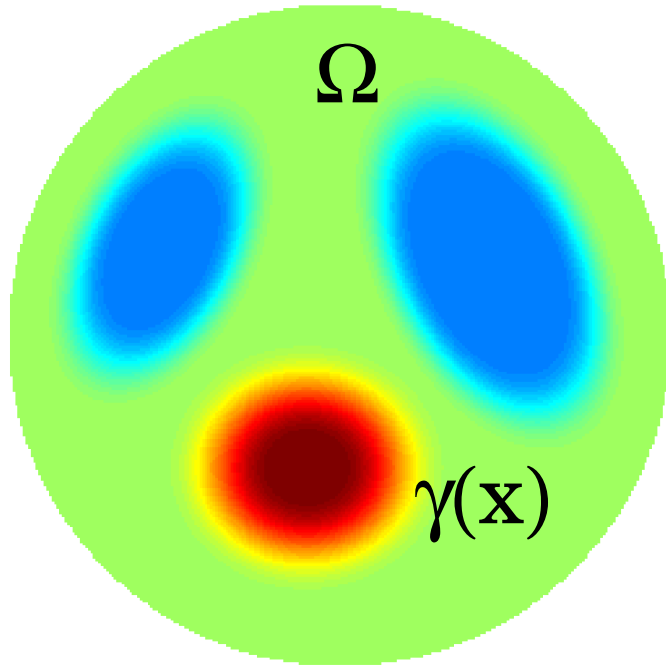
Feed electric currents through electrodes, measure voltages

Reconstruct the image of electric conductivity in a two-dimensional slice

Applications include:
monitoring heart and lungs of unconscious patients,
detecting pulmonary edema,
enhancing ECG and EEG



The inverse conductivity problem of Calderón is the mathematical model of EIT



$$\Lambda_\gamma f = \gamma \frac{\partial u}{\partial \nu} \Big|_{\partial \Omega},$$

$$\begin{aligned} \nabla \cdot \gamma \nabla u &= 0 \quad \text{in } \Omega, \\ u &= f \quad \text{on } \partial \Omega. \end{aligned}$$

We assume that $0 < c \leq \gamma(x) \leq C$ for all $x \in \Omega$.

Problem: given the Dirichlet-to-Neumann map,
how to reconstruct the conductivity?

The reconstruction problem is nonlinear and ill-posed.

EIT reconstruction algorithms can be divided roughly into the following classes:

Linearization

Iterative **regularization methods**

Statistical inversion

Resistor network method

Convexification method

Layer stripping

The inverse scattering approach, or the **d-bar method**

This is a brief history of regularization methods for electrical impedance tomography

- 1991 **Hua, Woo, Webster** and **Tompkins** (Tikhonov and smoothness)
- 1992 **Goble, Cheney** and **Isaacson** (truncated Newton method)
- 1994 **Dobson** and **Santosa** (Total variation)
- 1999 **Vauhkonen** et al. (Tikhonov in 3D)
- 2001 **Kindermann** and **Neubauer** (surface representation)
- 2001 **Rondi** and **Santosa** (Mumford-Shah-functional)
- 2003 **Lukaschewitsch, Maass** and **Pidcock** (Tikhonov regularization)
- 2005 **Chung, Chan** and **Tai** (level set, total variation)
- 2005 **Eppler** and **Harbrecht** (Newton regularization)
- 2006 **Lechleiter** and **Rieder** (numerical Newton regularization)
- 2008 **Rondi** (theory for regularized recovery of discontinuities)
- 2008 **Lechleiter** and **Rieder** (local convergence of Newton regularization)

This is a brief history of the development of the d-bar method in dimension two

Theory

1980 Calderón

1987 Sylvester and Uhlmann

1987 R G Novikov

1988 Nachman

1996 Nachman

1997 Liu

1997 Brown and Uhlmann

2001 Barceló, Barceló and Ruiz

2000 Francini

2003 Astala and Päivärinta

2007 Barceló, Faraco and Ruiz

2008 Clop, Faraco and Ruiz

Practice

2008 Bikowski and Mueller

2000 S, Mueller and Isaacson

2003 Mueller and S

2004 Isaacson, Mueller, Newell and S

2006 Isaacson, Mueller, Newell and S

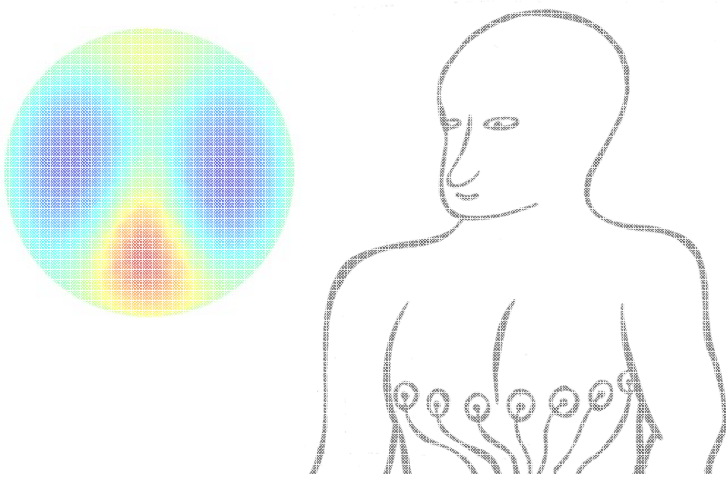
2007 Murphy

2008 Knudsen, Lassas, Mueller and S

2001 Knudsen and Tamasan

2003 Knudsen

2008 Astala, Mueller, Päivärinta and S



1. Electrical impedance tomography

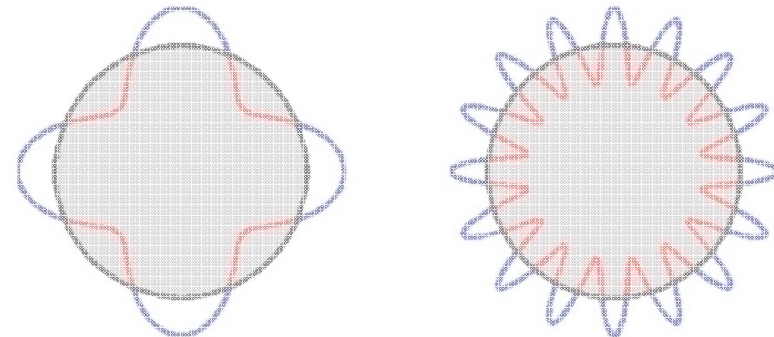
$$\frac{\partial}{\partial \bar{k}} \mu(x, k) = \frac{t(k)}{4\pi \bar{k}} e^{-i(kx + \bar{k}\bar{x})} \overline{\mu(x, k)}.$$

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3. Regularization results

$$\sup_{\Lambda_\gamma^\varepsilon} \{ \|\Gamma_{\alpha(\varepsilon)} \Lambda_\gamma^\varepsilon - \gamma\|_{L^\infty(\Omega)} : \|\Lambda_\gamma^\varepsilon - \Lambda_\gamma\|_Y \leq \varepsilon \}$$

4. Practical computation



Nachman's 1996 proof consists of two steps:

$$\Lambda_\gamma \longrightarrow \mathbf{t} \longrightarrow \gamma$$

The intermediate object \mathbf{t} is a complex-valued function called *scattering transform* and defined as follows:

$$\mathbf{t}(k) := \int_{\mathbb{R}^2} e^{i\bar{k}\bar{x}} q(x) \psi(x, k) dx$$

$$q = \frac{\Delta \gamma^{1/2}}{\gamma^{1/2}}$$

$$(-\Delta + q)\psi(\cdot, k) = 0$$

$$\psi(x, k) \sim e^{ikx} = e^{i(k_1 + ik_2)(x_1 + ix_2)}$$

Step 1: from DN map to scattering transform

Solve traces of ψ from the boundary integral equation

$$\psi(\cdot, k)|_{\partial\Omega} = e^{ikx} - S_k(\Lambda_\gamma - \Lambda_1)\psi(\cdot, k),$$

where the single-layer operator has Faddeev Green's function as kernel.

Compute the scattering transform as

$$\mathbf{t}(k) = \int_{\partial\Omega} e^{i\bar{k}\bar{x}} (\Lambda_\gamma - \Lambda_1)\psi(x, k) d\sigma(x).$$

Let us take a closer look at Faddeev Green's function and the related single layer operator

The operator

$$(S_k \phi)(x) := \int_{\partial\Omega} G_k(x - y) \phi(y) d\sigma(y)$$

involves the Faddeev Green's function G_k for the Laplacian:

$$-\Delta G_k(x) = \delta_0(x).$$

The function G_k can be written in the form

$$G_k(x) := e^{ikx} g_k(x),$$

where

$$g_k(x) := \frac{1}{(2\pi)^2} \int_{\mathbb{R}^2} \frac{e^{ix \cdot \xi}}{|\xi|^2 + 2k(\xi_1 + i\xi_2)} d\xi.$$

Step 2: from scattering transform to γ

Define $\mu(x, k) = e^{-ikx}\psi(x, k)$

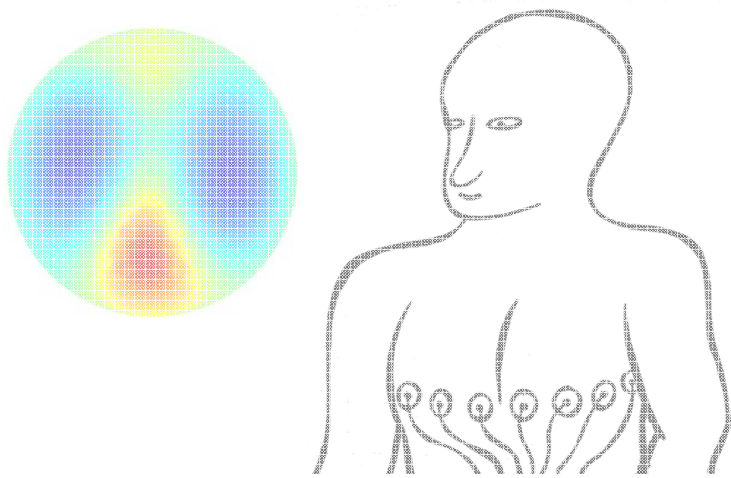
Then the following d-bar equation holds:

$$\frac{\partial}{\partial \bar{k}} \mu(x, k) = \frac{t(k)}{4\pi \bar{k}} e^{-i(kx + \bar{k}\bar{x})} \overline{\mu(x, k)}.$$

Here $\frac{\partial}{\partial \bar{k}} = \frac{1}{2} \left(\frac{\partial}{\partial k_1} + i \frac{\partial}{\partial k_2} \right)$.

The d-bar equation has a unique solution for all x .
The conductivity can be recovered from

$$\gamma^{1/2}(x) = \lim_{k \rightarrow 0} \mu(x, k).$$



1. Electrical impedance tomography

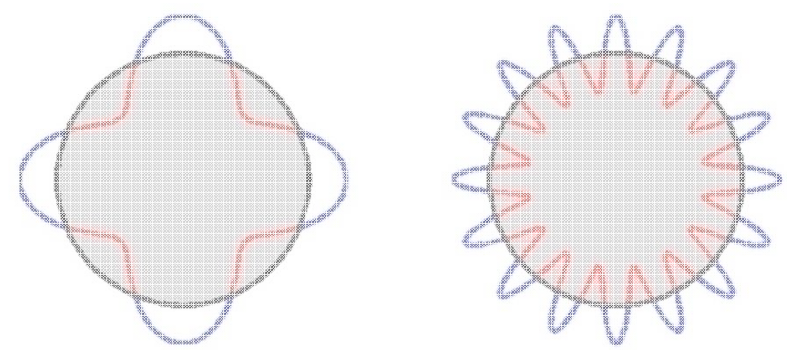
$$\frac{\partial}{\partial \bar{k}} \mu(x, k) = \frac{t(k)}{4\pi \bar{k}} e^{-i(k\bar{a} + \bar{k}a)} \mu(x, k).$$

2. Theory of the D-bar method

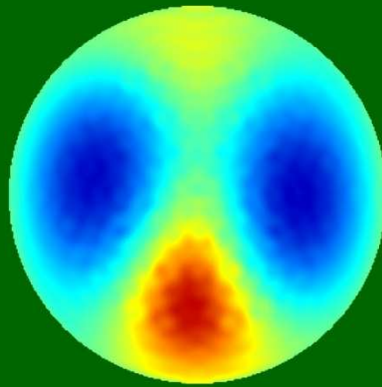
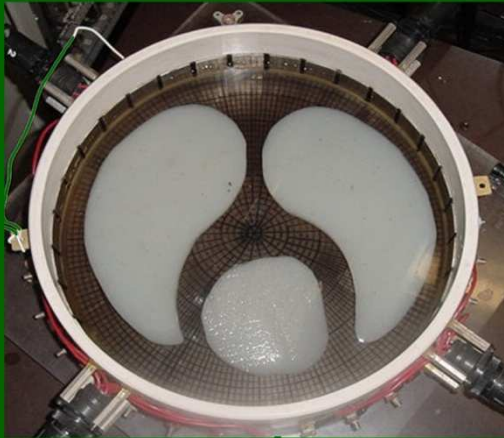
3. Regularization results

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4. Practical computation



We have achieved excellent EIT reconstructions from practical data (phantom and *in vivo* human) using Born approximation to linearize Step 1.



However, that approach does not allow regularization analysis.

We work within the following assumptions:

Let $\Omega \subset \mathbb{R}^2$ be the open unit disc.

Define the forward map F between the spaces

$$F : \mathcal{D}(F) \subset L^\infty(\Omega) \rightarrow Y.$$

Domain $\mathcal{D}(F)$ is defined as follows.

Let $M > 0$ and $0 < \rho < 1$. The set $\mathcal{D}(F)$ contains functions $\gamma : \Omega \rightarrow \mathbb{R}$ satisfying

$$(a) \quad \|\gamma\|_{C^2(\overline{\Omega})} \leq M,$$

$$(b) \quad \gamma(x) \geq M^{-1} \text{ for all } x \in \Omega,$$

$$(c) \quad \gamma(x) \equiv 1 \text{ for } \rho < |x| < 1.$$

Space Y of data is defined as follows.

Y consists of bounded linear operators

$$\Lambda : H^{1/2}(\partial\Omega) \rightarrow H^{-1/2}(\partial\Omega)$$

satisfying $\int_{\partial\Omega} \Lambda(f) d\sigma = 0$ and $\Lambda(1) = 0$.

Let us emphasize one of the strengths of our new results

Conditional stability results have the form

$$\|\gamma_1 - \gamma_2\|_Z \leq f(\|\Lambda_{\gamma_1} - \Lambda_{\gamma_2}\|_Y),$$

where γ_1, γ_2 belong to some function space Z and f is a continuous function with $f(0) = 0$.

The above estimate is not practically relevant.

The noisy measurement $\Lambda_{\gamma}^{\varepsilon}$ is in general not the DN map of some conductivity.

In contrast, we prove regularization properties for the D-bar method under the practically feasible assumption $\|\Lambda_{\gamma}^{\varepsilon} - \Lambda_{\gamma}\|_Y \leq \varepsilon$.

Let us define nonlinear regularization strategy (following Engl, Hanke & Neubauer and Kirsch)

Recall direct problem: $\gamma \in X$ maps to $\Lambda_\gamma \in Y$.

A family of continuous mappings $\Gamma_\alpha : Y \rightarrow X$ with $0 < \alpha < \infty$ is a **regularization strategy** if

$$\lim_{\alpha \rightarrow 0} \|\Gamma_\alpha \Lambda_\gamma - \gamma\|_{L^\infty(\Omega)} = 0$$

for each fixed $\gamma \in X$. A regularization strategy with a choice $\alpha = \alpha(\varepsilon)$ is called **admissible** if

$$\alpha(\varepsilon) \rightarrow 0 \text{ as } \varepsilon \rightarrow 0,$$

and for any fixed $\gamma \in X$ the following holds:

$$\sup_{\Lambda_\gamma^\varepsilon} \left\{ \|\Gamma_{\alpha(\varepsilon)} \Lambda_\gamma^\varepsilon - \gamma\|_{L^\infty(\Omega)} : \|\Lambda_\gamma^\varepsilon - \Lambda_\gamma\|_Y \leq \varepsilon \right\} \xrightarrow{\varepsilon \rightarrow 0} 0.$$

This is our regularized D-bar method for EIT

Given the noise level $\varepsilon > 0$, solve the equation

$$\psi^\varepsilon(\cdot, k)|_{\partial\Omega} = e^{ikx} - S_k(\Lambda_\gamma^\varepsilon - \Lambda_1)\psi^\varepsilon(\cdot, k)|_{\partial\Omega}$$

for $|k| < R(\varepsilon) := -\frac{1}{10} \log(\varepsilon)$.

Introduce nonlinear low-pass filtering

$$\mathbf{t}_R^\varepsilon(k) := \begin{cases} \int_{\partial\Omega} e^{i\bar{k}\bar{x}} (\Lambda_\gamma^\varepsilon - \Lambda_1)\psi^\varepsilon(\cdot, k) d\sigma & \text{for } |k| < R(\varepsilon), \\ \text{zero} & \text{for } |k| \geq R(\varepsilon). \end{cases}$$

For each $x \in \Omega$, solve the integral equation

$$\mu_R(x, k) = 1 + \frac{1}{(2\pi)^2} \int_{\mathbb{R}^2} \frac{\mathbf{t}_R^\varepsilon(s)}{(k-s)\bar{s}} e^{-x(s)} \overline{\mu_R(x, s)} ds_1 ds_2,$$

and define $\alpha(\varepsilon) = \frac{1}{R(\varepsilon)}$ and $(\Gamma_\alpha \Lambda_\gamma^\varepsilon)(x) := (\mu_R(x, 0))^2$.

Theorem [Knudsen, Lassas, Mueller & S 2008]

The family Γ_α is well-defined for small $\alpha > 0$. It is an admissible regularization strategy with

$$\alpha(\varepsilon) = \left(-\frac{1}{10} \log(\varepsilon)\right)^{-1}.$$

Furthermore, we have the explicit estimate

$$\sup_{\Lambda_\gamma^\varepsilon} \left\{ \|\Gamma_{\alpha(\varepsilon)} \Lambda_\gamma^\varepsilon - \gamma\|_{L^\infty(\Omega)} : \|\Lambda_\gamma^\varepsilon - \Lambda_\gamma\|_Y \leq \varepsilon \right\}$$

$$\leq C(-\log \varepsilon)^{-1/14}$$

$$\rightarrow 0 \text{ as } \varepsilon \rightarrow 0.$$

Proof of the main theorem is divided into several lemmata. First a D-bar estimate:

Lemma 1. Let $4/3 < r_0 < 2$ and suppose that $\phi_1, \phi_2 \in L^r(\mathbb{R}^2)$ for all $r \geq r_0$. Let μ_1, μ_2 , be the solutions of

$$\mu_j(x, k) = 1 + \frac{1}{(2\pi)^2} \int_{\mathbb{R}^2} \frac{\phi_j(k')}{(k - k')} \overline{\mu_j(x, k')} dk'_1 dk'_2,$$

$j = 1, 2$. Then for fixed $x \in \overline{\Omega}$ we have

$$\|\mu_1(x, \cdot) - \mu_2(x, \cdot)\|_{C^\alpha(\mathbb{R}^2)} \leq C \|\phi_1 - \phi_2\|_{L^{r_0} \cap L^{r_0'}(\mathbb{R}^2)},$$

where $\alpha < 2/r_0 - 1$ and $1/r_0' = 1 - 1/r_0$.

Proof. Combination of well-known results.

These results follow from careful analysis of Faddeev's Green function

Lemma 2. Let $\phi_0 \in H^{-1/2}(\partial\Omega)$ with $\int \phi_0 = 0$. Then we have the estimate

$$\|S_k \phi_0\|_{H^{1/2}(\partial\Omega)} \leq C e^{2|k|} (1 + |k|) \|\phi_0\|_{H^{-1/2}(\partial\Omega)}.$$

Lemma 3. For $k \in \mathbb{C}$ we have the estimate

$$\left\| [I + S_k(\Lambda_\gamma - \Lambda_1)]^{-1} \right\|_{L(H^s(\partial\Omega))} \leq C_2 e^{2|k|} (1 + |k|),$$

where C_2 depends only on M and ρ .

Combining previous results, a perturbation argument, and delicate L^p analysis shows

Lemma 4. There exists $\varepsilon_0 > 0$, depending only on M and ρ , such that equation

$$\psi^\varepsilon(\cdot, k)|_{\partial\Omega} = e^{ikx} - S_k(\Lambda_\gamma^\varepsilon - \Lambda_1)\psi^\varepsilon(\cdot, k)|_{\partial\Omega}$$

is solvable in $H^{1/2}(\partial\Omega)$ for all $0 < \varepsilon \leq \varepsilon_0$ and $|k| < R$ with

$$R = R(\varepsilon) = -\frac{1}{10} \log \varepsilon.$$

Furthermore, for $p > 1$ we have the estimate

$$\left\| \frac{\mathbf{t}(k) - \mathbf{t}_R^\varepsilon(k)}{\bar{k}} \right\|_{L^p(|k| \leq R)} \leq C \varepsilon^{1/10} \left(-\frac{1}{10} \log \varepsilon \right)^{2/p},$$

where C is independent of p and R and ε .

Sketch of proof of main theorem

(i) $\lim_{\alpha \rightarrow 0} \|\Gamma_\alpha \Lambda_\gamma - \gamma\|_{L^\infty(\Omega)} = 0$ for $\gamma \in X$.

(ii) $\alpha(\varepsilon) \rightarrow 0$ as $\varepsilon \rightarrow 0$,

(iii) $\sup_{\Lambda_\gamma^\varepsilon} \left\{ \|\Gamma_{\alpha(\varepsilon)} \Lambda_\gamma^\varepsilon - \gamma\|_{L^\infty(\Omega)} : \|\Lambda_\gamma^\varepsilon - \Lambda_\gamma\|_Y \leq \varepsilon \right\}$
tends to zero as $\varepsilon \rightarrow 0$.

Claim (i) follows from [Nachman 1996] (with delicate choices of L^p spaces) and Lemma 1.
Claim (ii) is OK: $\alpha(\varepsilon) = \frac{1}{R(\varepsilon)} = -10(\log \varepsilon)^{-1}$.

Sketch of proof of main theorem

To prove that

$$\sup_{\Lambda_\gamma^\varepsilon} \left\{ \|\Gamma_{\alpha(\varepsilon)} \Lambda_\gamma^\varepsilon - \gamma\|_{L^\infty(\Omega)} : \|\Lambda_\gamma^\varepsilon - \Lambda_\gamma\|_Y \leq \varepsilon \right\}$$

tends to zero as $\varepsilon \rightarrow 0$ we combine [Nachman 1996] with Lemmata 1 and 4 to estimate

$$\begin{aligned} & \|\mu(x, \cdot) - \mu_R(x, \cdot)\|_{C^\alpha(\mathbb{R}^2)} \\ & \leq C \left\| \frac{\mathbf{t}(k) - \mathbf{t}_R^\varepsilon(k)}{\bar{k}} \right\|_{L^p \cap L^{p'}(\mathbb{R}^2)} \\ & \leq C \left\| \frac{\mathbf{t}(k) - \mathbf{t}_R^\varepsilon(k)}{\bar{k}} \right\|_{L^p \cap L^{p'}(|k| < R)} + C \left\| \frac{\mathbf{t}(k)}{\bar{k}} \right\|_{L^p(|k| > R)} \\ & \leq C \left(-\frac{1}{10} \log \varepsilon\right)^{10/7} \varepsilon^{1/10} + CR(\varepsilon)^{-\frac{1}{7}} + CR(\varepsilon)^{-\frac{1}{14}} \\ & = C(-\log \varepsilon)^{10/7} \varepsilon^{1/10} + C(-\log \varepsilon)^{-\frac{1}{7}} + C(-\log \varepsilon)^{-\frac{1}{14}}. \end{aligned}$$

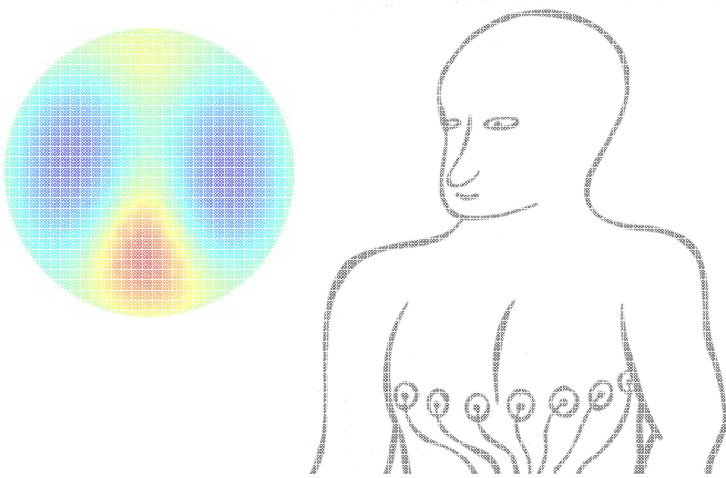
One more thing: the regularization strategy is not yet defined on all of data space Y

The range $F(\mathcal{D}(F)) \subset Y$ is not known, and its structure may be complicated.

(This is related to the open and notoriously difficult *characterization problem*.)

The previous results show the claim only for operators ε_0 -close to the range $F(\mathcal{D}(F))$.

The problem can be overcome using spectral theoretical arguments.



1. Electrical impedance tomography

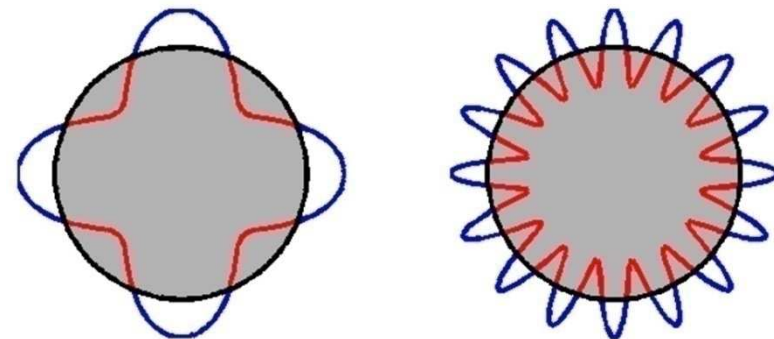
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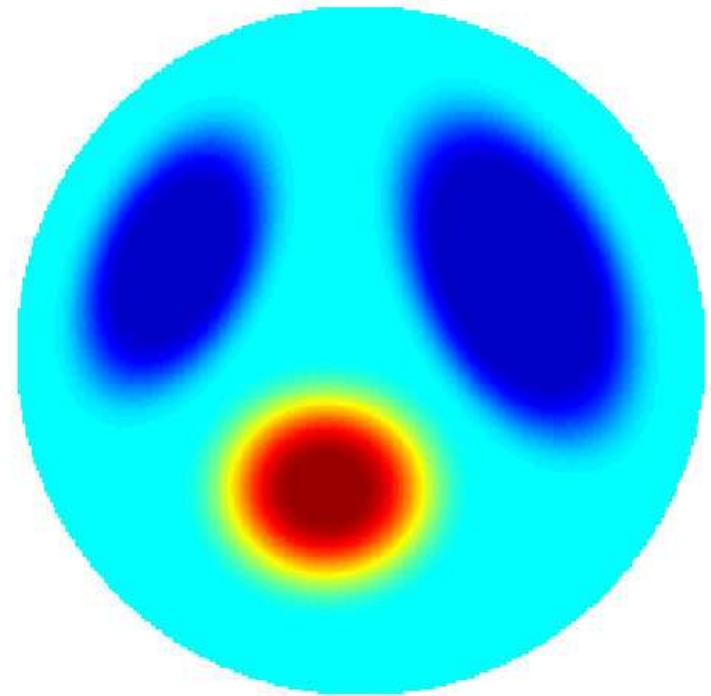
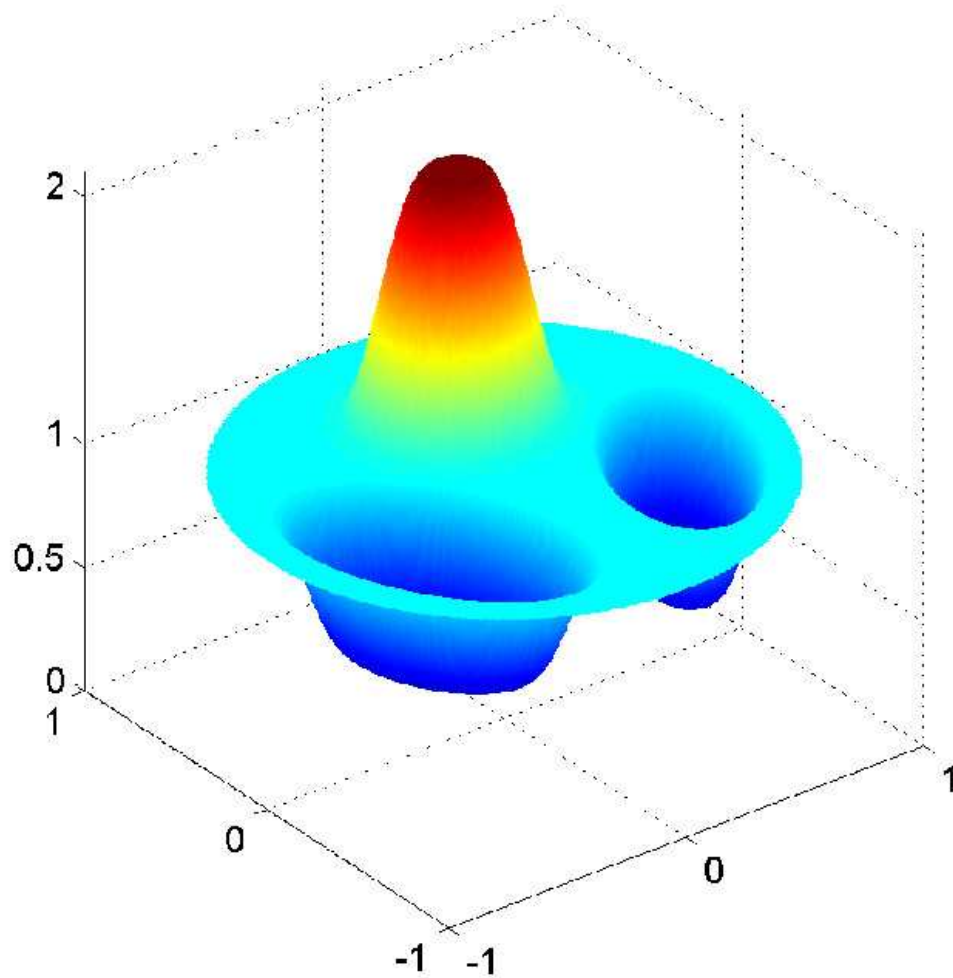
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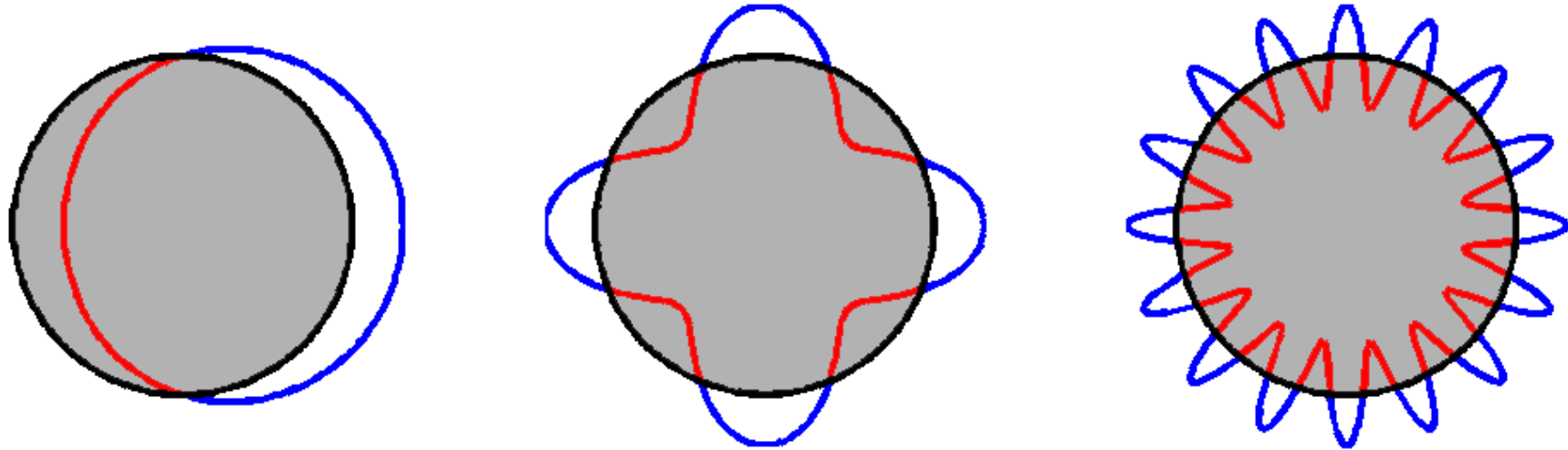
4. Practical computation



We construct a simulated human chest phantom for numerical testing



We use the truncated Fourier basis $\{e^{in\theta}\}_{n=-N}^N$ to express functions defined on the unit circle.



Integral operators $A : H^s(\partial\Omega) \rightarrow H^r(\partial\Omega)$ are represented as finite matrices $[\langle Ae^{in\theta}, e^{im\theta} \rangle]$.

- Λ_1 we know analytically,
- Λ_γ we compute using Finite Element Method,
- S_k we evaluate by numerical integration.

This is our practical two-step regularized D-bar method for EIT

1. We solve for $|k| < R$ the matrix version of

$$\psi^\varepsilon(\cdot, k)|_{\partial\Omega} = e^{ikx} - S_k(\Lambda_\gamma^\varepsilon - \Lambda_1)\psi^\varepsilon(\cdot, k)|_{\partial\Omega}$$

with R as large as numerically stable.

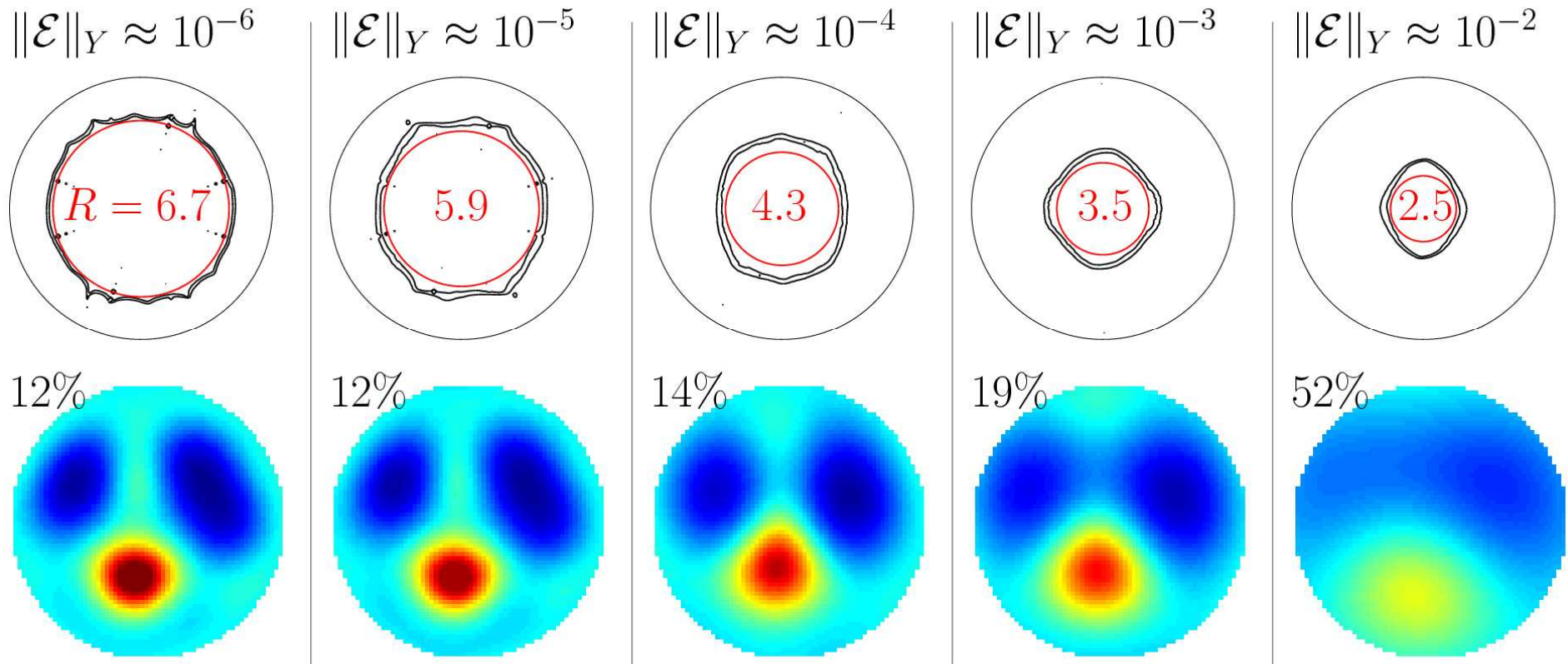
2. The integral equation

$$\mu_R(x, k) = 1 + \frac{1}{(2\pi)^2} \int_{\mathbb{R}^2} \frac{t_R^\varepsilon(s)}{(k-s)\bar{s}} e^{-x(s)} \overline{\mu_R(x, s)} ds_1 ds_2$$

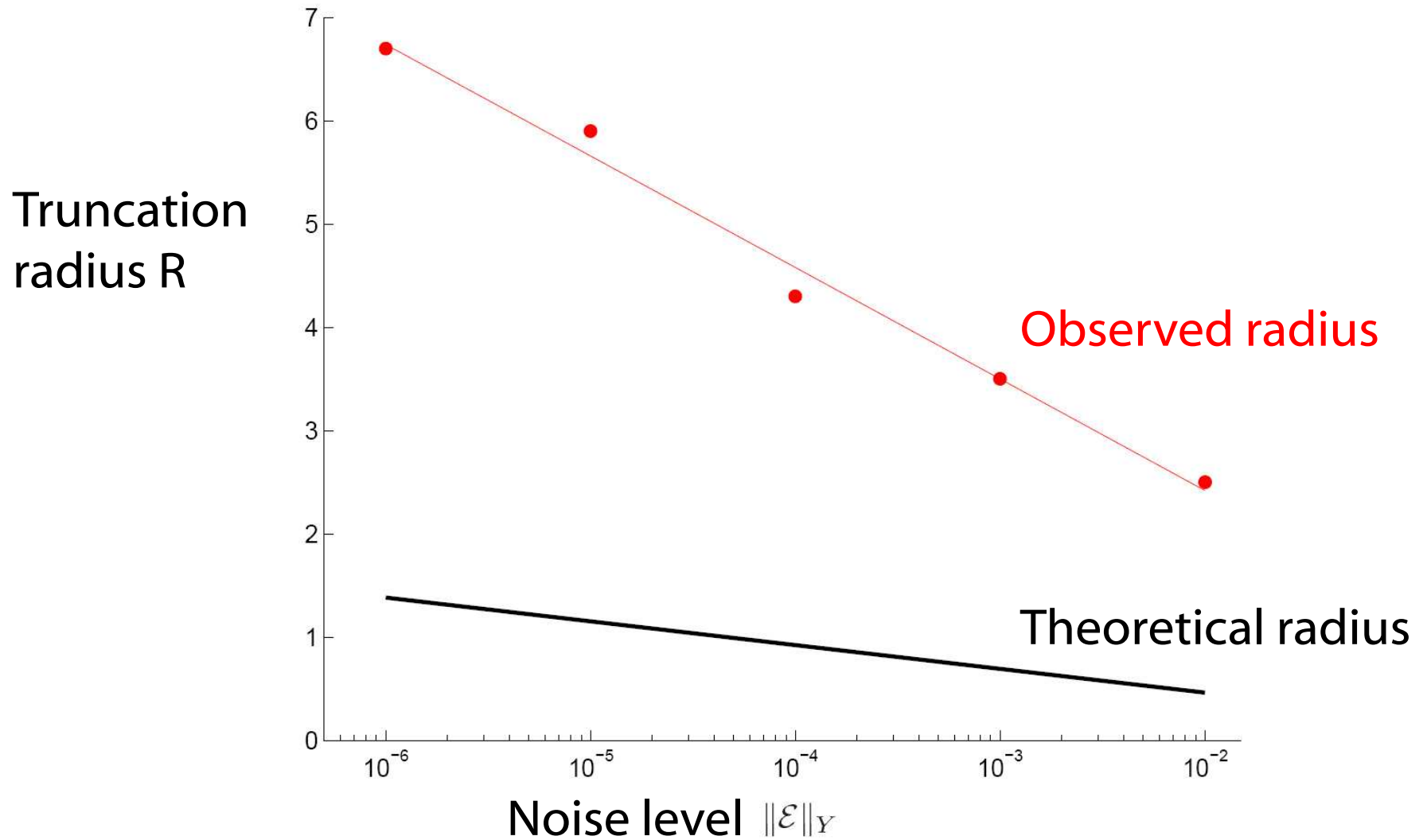
can be solved by our established D-bar solver.

The reconstructed conductivity is $\mu_R(x, 0)$.

Here we see the reconstructions corresponding to various levels of measurement noise



The numerical results actually improve the exponential behaviour predicted by theory



Thank you!

Preprints available at
www.siltanen-research.net

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